



# Direct laser writing of micropillars on Siloxane moulds for microrreplication

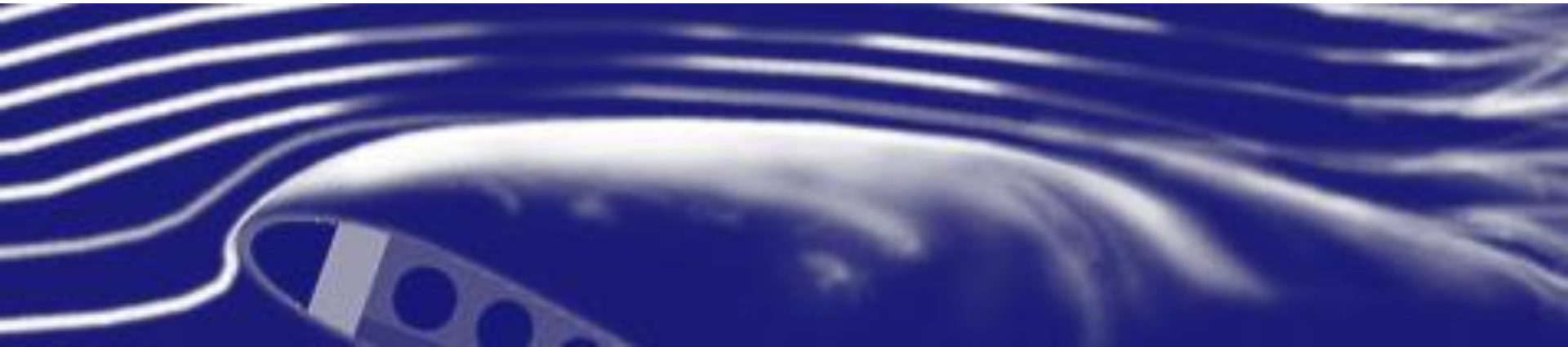


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- Motivation
- Laser direct writing of micromoulds in PDMS
- Replication results
- Conclusions and further work



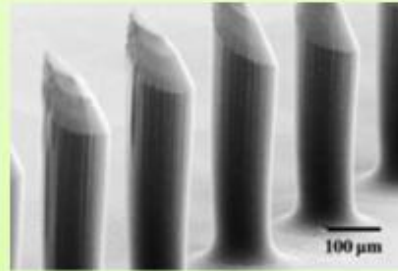
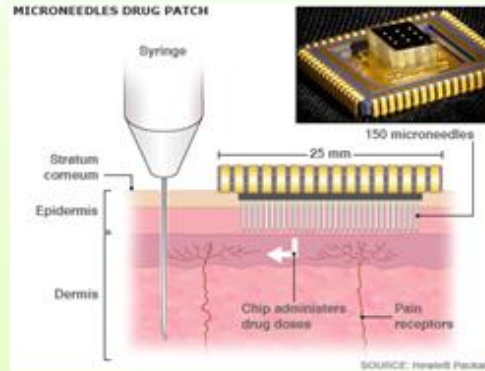
# Motivation



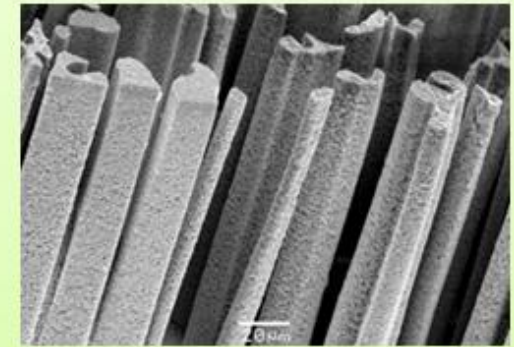
## THREE INNOVATIVE PRODUCT DESIGNS: Microfluidics, microneedles, piezotransducers.



Handheld analyzer and  
Microfluidic chip (SensLab)



Drug Patch Chip and  
microneedle array (Crospon)



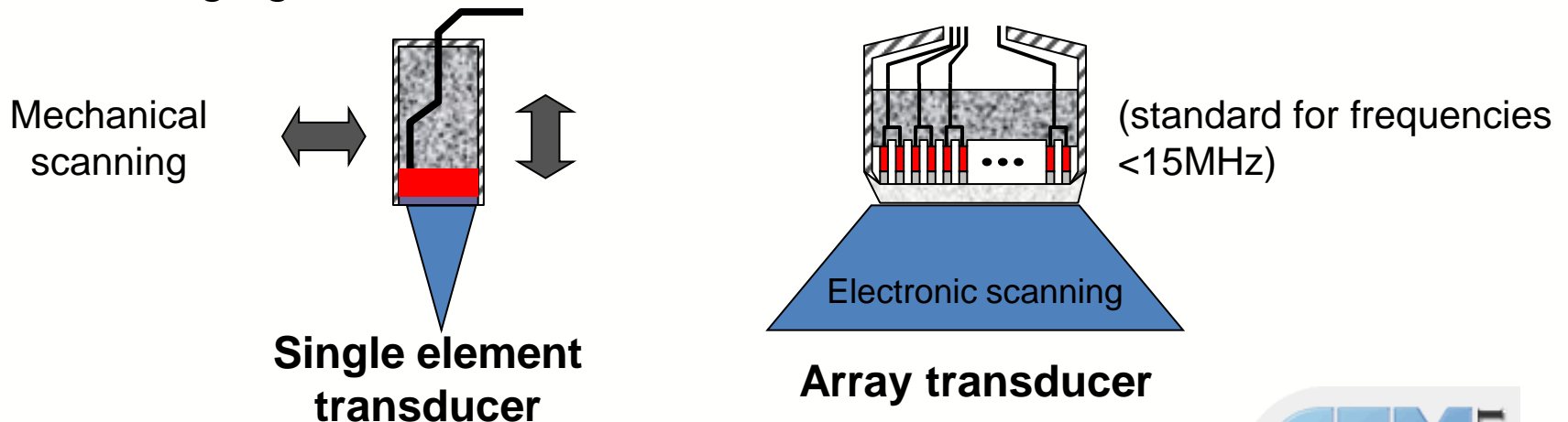
IntraVenous US Catheter and  
microPTZ transducer (AFM)

## Manufacturing challenges:

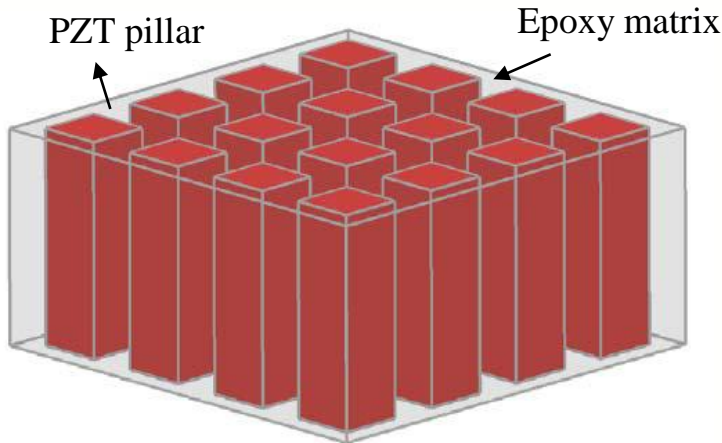
- Integration of functional and disposable parts: need for “functional materials and geometries”
- Manufacturing cost and flexibility: Disposable part of the device need very low cost. Patient sp.

## Ultrasound Technology

- Safe, inexpensive, real time - >20% of all clinical scans (\$5bn).
- Widely used in Fetal imaging, Cardiac imaging, Blood flow measurement, Intra-operative guidance.
  - Utilises machined piezoelectric ceramic element
  - Minimum image feature size 150um at 10MHz
  - Current commercial limit ~15MHz.
- For imaging:



# 1-3 piezocomposites

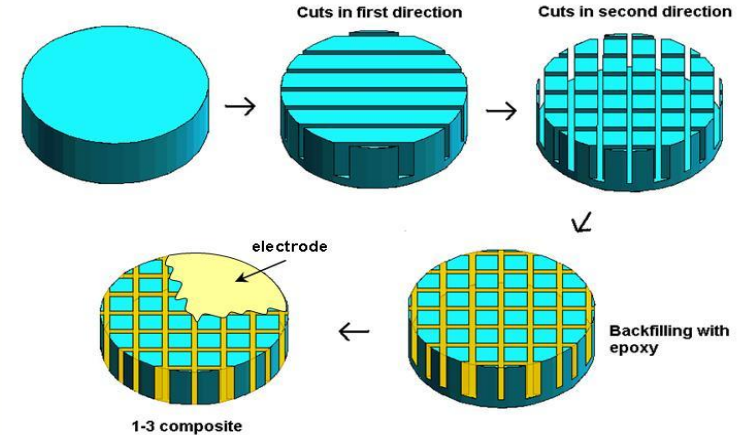


1-3 piezocomposite

## Dimension requirements

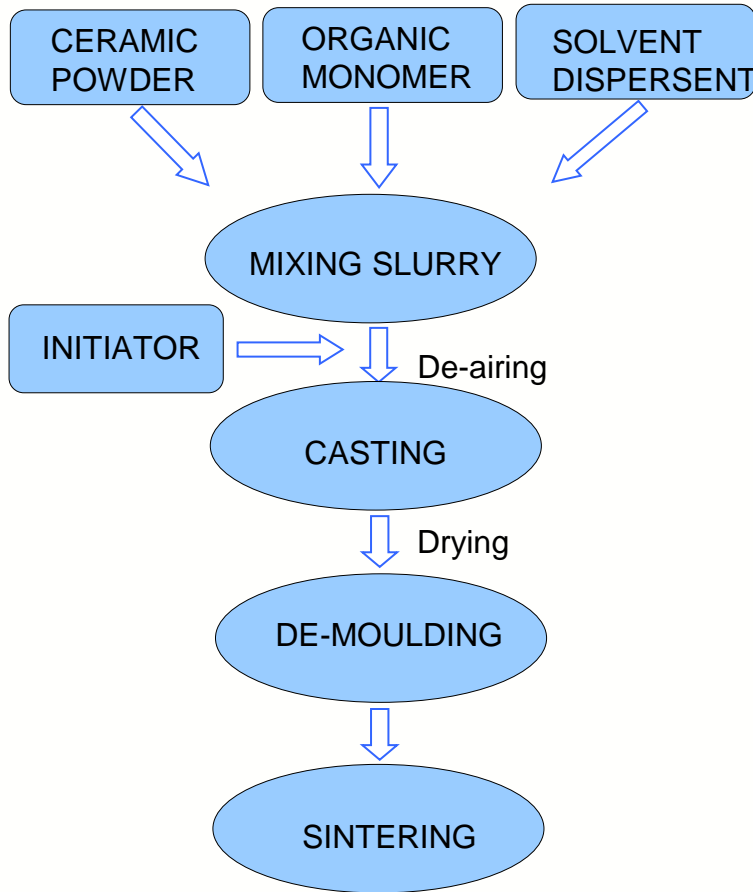
Frequency	20 MHz	40 MHz
Pillar width	24 $\mu\text{m}$	14 $\mu\text{m}$
Kerf	20 $\mu\text{m}$	8 $\mu\text{m}$
Thickness	80 $\mu\text{m}$	40 $\mu\text{m}$

- Piezocomposites made almost exclusively by the dice-and-fill technique for  $f < 20\text{MHz}$
- Impossible to fabricate high frequency arrays by dice and fill because of the ultrafine feature size required.



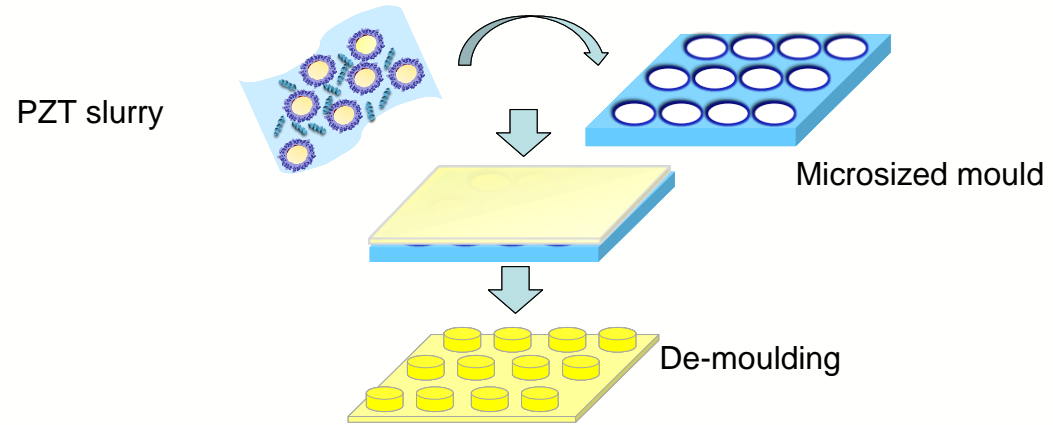
Conventional dice-and-fill technique

Current transducer manufacturing techniques limit frequency to  $< 15\text{MHz}$ , thus limited resolution.

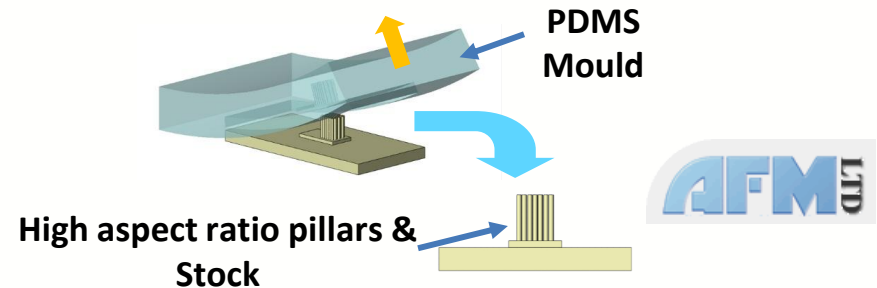


Flow chart of gel casting process.

- Capability of producing complex parts
- Homogeneous material properties
- Rapid forming cycle
- Low capital equipment cost.



Gel casting for 1-3 piezocomposite fabrication.



**Material:** Etched silicon master pattern is replicated on PDMS (later used to cast the ceramic slurry);



## Direct laser fabrication of PDMS moulds

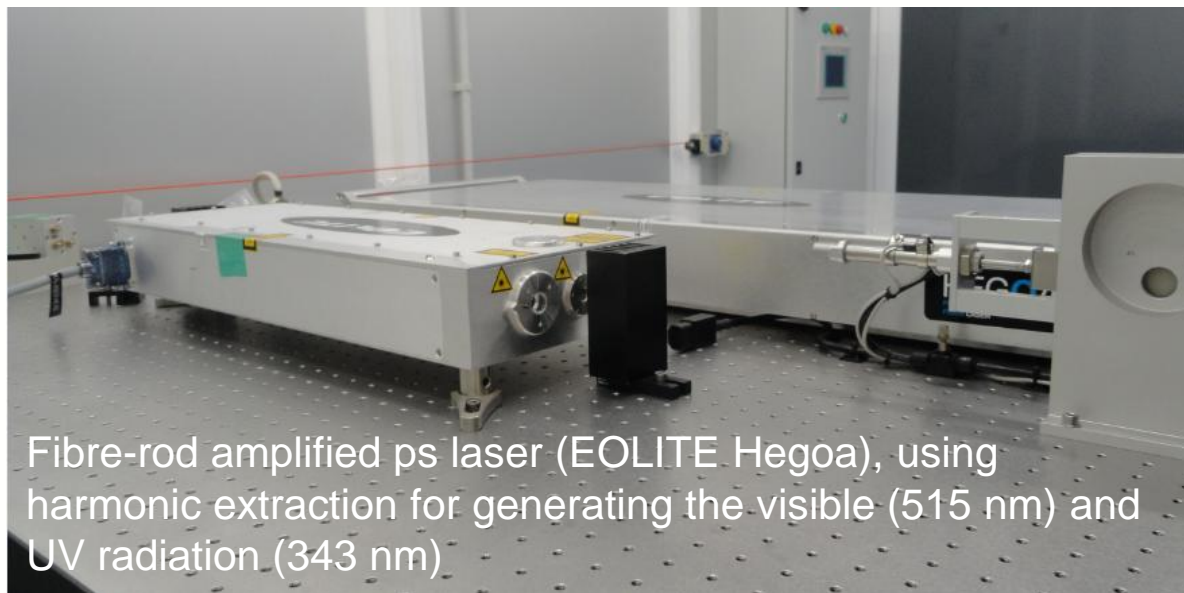




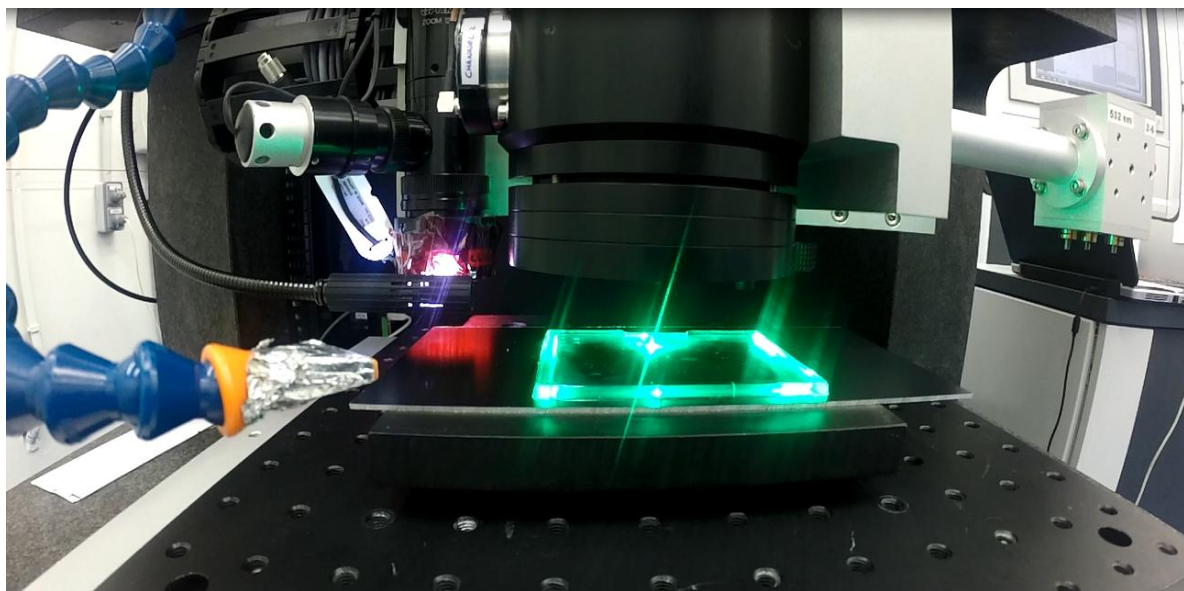


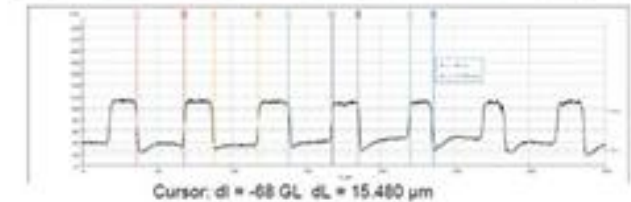
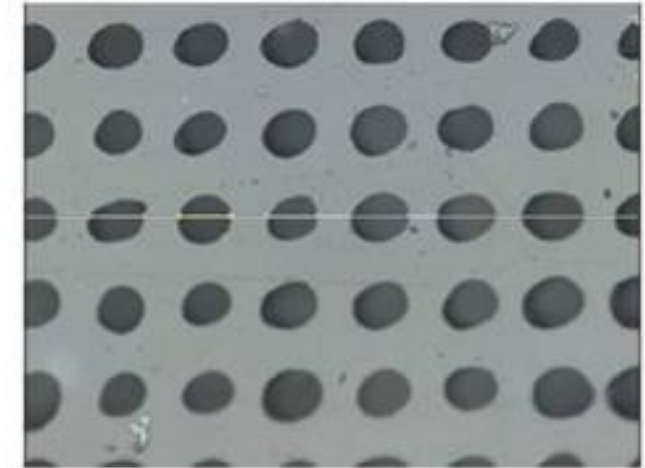
The laser beam is focused with:

- Microscope objective lens (20x with  $NA=0.4$ ).
- 35 mm focal length flat field optics (Theta-lens),  $NA=0.15$ .



Fibre-rod amplified ps laser (EOLITE Hegoa), using harmonic extraction for generating the visible (515 nm) and UV radiation (343 nm)





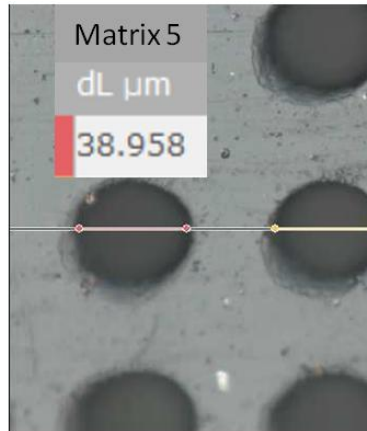
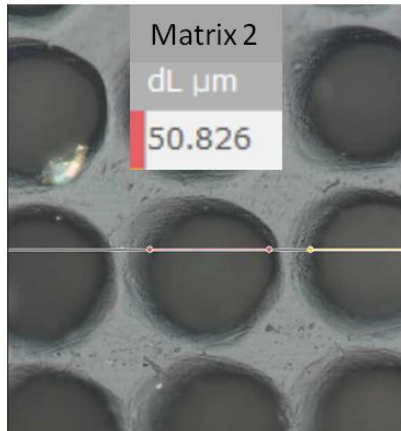
Patterned moulds on 2mm x 2mm area

Repetition rates around 1 MHz provide good quality and well controlled hole diameter.

10  $\mu\text{J}$  per pulse,  
focal spot of 15  $\mu\text{m}$   
30 ps of pulse duration

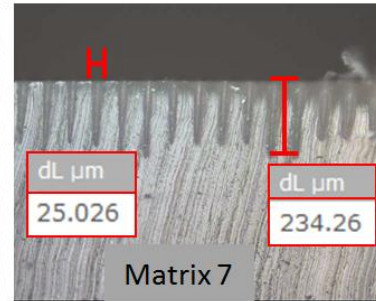
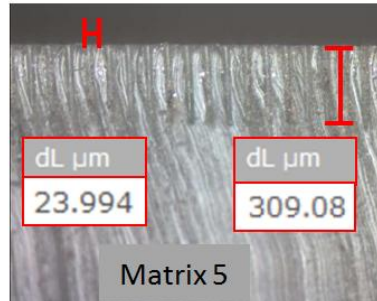
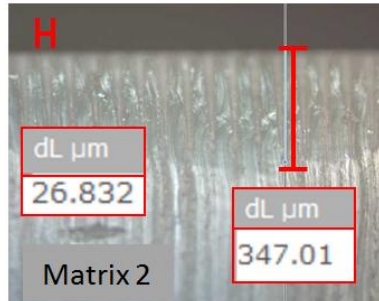
For higher repetition rates, or higher pulse energies, the laser produces widening of the micro-channel diameter, and particularly larger distortion and widening of the entrance diameter.

Below 1 MHz did not improve the process with either poor or no PDMS ablation.



Hole highly dependent on laser pulse characteristics.

7 % increase in the pulse energy results in a considerable increase in the drilled depth and larger dispersion



Diameter enlarged with higher power

Processing window relatively narrow

	Energy (μJ)	Avg. Depth (μm)	St. Dev. (μm)	Diam (μm)
Matrix: M5	8.4	289.5	15.0	38.4
Matrix: M2	9.6	358.7	54.5	52.5

35 – 40 micro channels per second

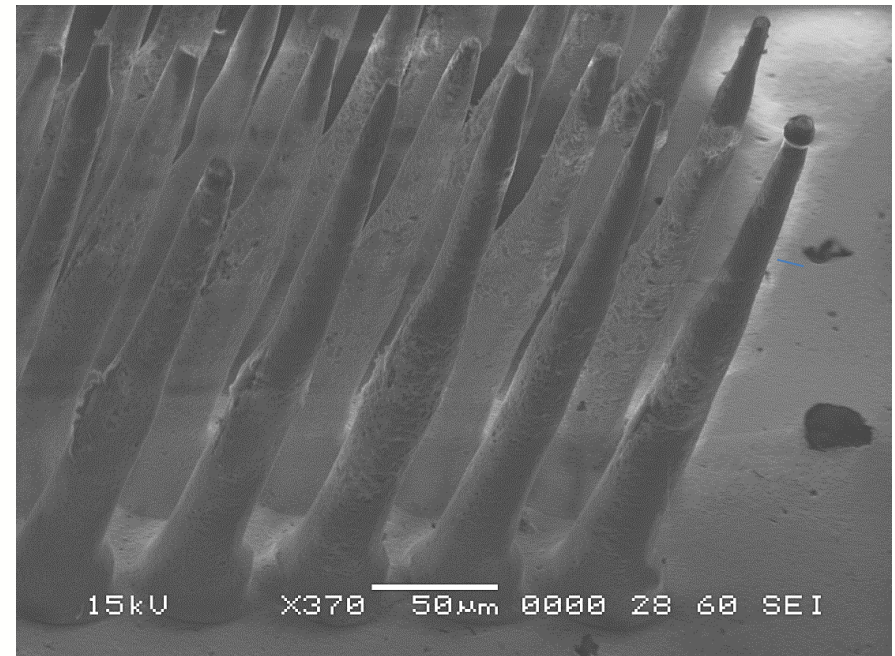
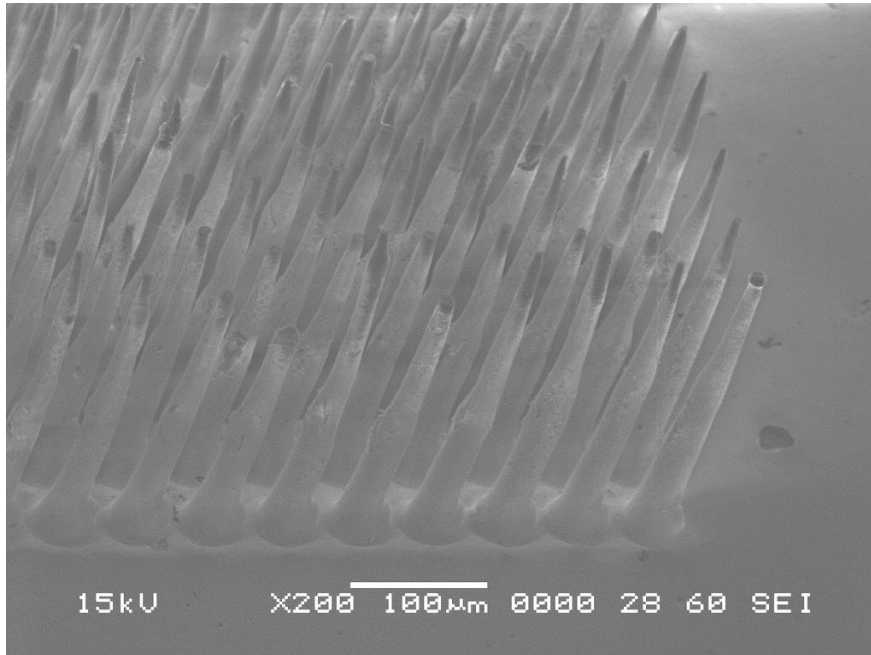


## Replication results



# De-moulded green pillar structure

For assessment of the channel matrix quality and correct geometry, the fabricated moulds were used for replication via epoxy gel casting of PZT slurry (0.8  $\mu\text{m}$  particle size, 45% vol. solid fraction, 40% epoxy).



## Pillar geometry:

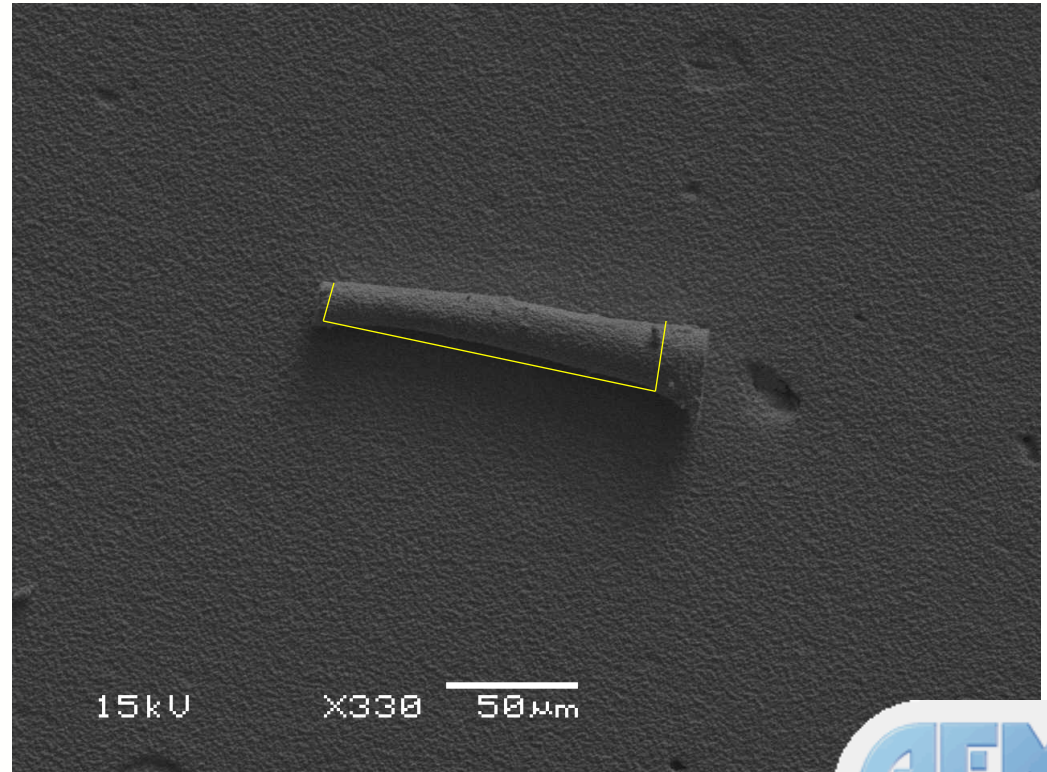
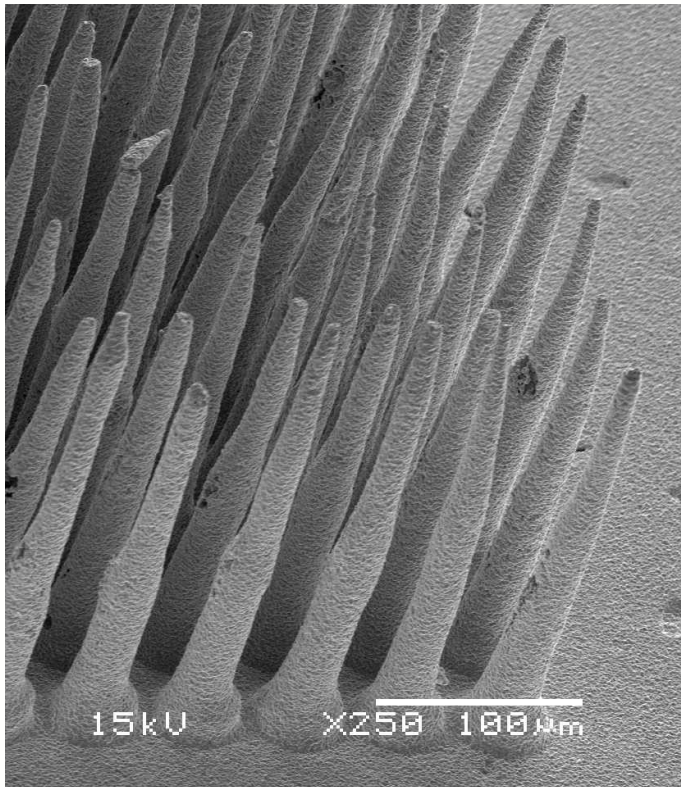
Fine tips (bottom of the laser drilled channel, diameter  $\sim 32\mu\text{m}$ )

Cylindrical section (base: opening of the hole in the surface,  $\sim 43\mu\text{m}$  diameter)

Pillar height:  $>180$  microns

Tips irregular and with inconsistent height → structures encapsulated in polymer and lapped

→ 125 microns of usable portion, cylindrical, with 5 degrees taper



# FABIMED PROJECT

FABRICATION AND FUNCTIONALIZATION OF BIOMEDICAL MICRODEVICES



## Acknowledgement



The work leading to the results enclosed in this paper, has received funding from the European Union Seventh Framework Programme FP7/2007-2013 under grant agreement n° 608901, FaBiMed project: “Fabrication and functionalization of biomedical microdevices”.

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**Thank you!**

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